

# 1 Gait and Balance Function Improves After 10 Weeks of Using a 2 Wearable Sensory Neuroprosthesis in Persons with Peripheral 3 Neuropathy and High Fall Risk – the walk2Wellness Trial

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18

## 19 Abstract

20 **Background:** Patients with sensory peripheral neuropathy (PN) commonly present with gait and balance  
21 problems increasing their risk of falls. The multi-site walk2Wellness trial investigates effects of long-term,  
22 home-based daily use of a wearable lower limb sensory neuroprosthesis on gait function, balance, quality of  
23 life and fall rates in a cohort of PN patients. The device (Walkasins®, RxFunction Inc., MN, USA) is designed  
24 to replace lost nerve function related to foot pressure sensation by providing directional tactile cues around the  
25 ankle reflecting foot pressure measurements during standing and walking activities. We hypothesized that  
26 previously shown short-term in-clinic improvements in gait and balance would be sustained after 10 weeks of  
27 use.

28 **Methods:** Participants had a PN diagnosis with loss of plantar sensation associated with gait and balance  
29 problems, a Functional Gait Assessment (FGA) score <23 (cut-off for high fall risk), and ability to sense Leg  
30 Unit tactile stimuli. Clinical outcomes included FGA, Gait Speed, Timed Up&Go (TUG) and Four-Stage  
31 Balance Test. Patient-reported outcomes included Activities-Specific Balance Confidence (ABC) scale,  
32 Vestibular Disorders Activities of Daily Living Scale (VADL), PROMIS participation and satisfaction scores,  
33 pain rating, and falls. Evaluations were performed at baseline visit and after 2, 6, and 10 weeks. Subjects were  
34 not made aware of any changes in outcomes and no additional balance interventions were allowed.

35 **Results:** Forty-five participants of 52 enrolled across four sites completed all in-clinic assessments. FGA  
36 scores improved from 15.0 at baseline to 19.1 at 10 weeks ( $p<0.000001$ ), normal and fast gait speed from  
37 0.86m/s to 0.95m/s ( $p<0.00005$ ) and 1.24m/s to 1.33m/s ( $p<0.002$ ), respectively, and TUG from 13.8s to 12.5s  
38 ( $p<0.012$ ). Four-Stage Balance Test did not improve significantly. Several patient-reported outcomes were in  
39 normal range at baseline and remained largely unchanged. Interestingly, while FGA scores improved similarly  
40 across the baseline range, subjects with baseline ABC scores lower than 67% (cut-off for high fall risk)  
41 showed an increase in their ABC scores (from 49.9% to 59.3%,  $p<0.01$ ), whereas subjects with baseline ABC  
42 scores above 67% showed a decrease (from 76.6% to 71.8%,  $p<0.019$ ). Subjects who reported falls in the prior  
43 six months ( $n=25$ ) showed a decrease in the number of fall-risk factors (from 5.1 to 4.3,  $p<0.023$ ) as well as a  
44 decrease in fall rate from 13.8 to 7.4 falls/1000 days ( $p<0.014$ ). Four subjects in the pre-study non-faller group  
45 ( $n=20$ ) fell during the 10 weeks of the study.

46 **Conclusion:** A wearable sensory neuroprosthesis may provide a new way to treat gait and balance problems  
47 and manage falls in high fall-risk patients with PN.

48 **Trial registration:** ClinicalTrials.gov (#NCT03538756)

49

50 **Keywords:** Peripheral Neuropathy, Falls, Neuroprosthesis, Balance, Gait Speed, Function,  
51 Neuromodulation, Clinical Trial

52

## 53 1 Introduction

54 Falls are a widely recognized problem in the elderly (Ganz and Latham, 2020). About 29% of  
55 community-dwelling adults 65 years or older fall once annually and 10% fall at least twice annually  
56 (Ganz et al., 2007; Bergen et al., 2016). Data from the Centers for Disease Control (CDC) indicate  
57 that medical treatment was required by 37.5% of individuals who fell in 2014 (Bergen et al., 2016).  
58 Sterling et al. (Sterling et al., 2001) reported that 30% of falls in the elderly result in serious injury. In  
59 2015, medical cost related to fatal and nonfatal falls was approximately \$50.0 billion (Florence et al.,  
60 2018). Overall, falls are associated with poor health, shortened survival (Jónsdóttir and Ruthig,  
61 2020), reduced quality of life, and a fear of falling (Lawrence et al., 1998; Scheffer et al., 2008).  
62 Sensory peripheral neuropathy (PN) is associated with poor balance and is an independent risk factor  
63 for falls (Richardson and Hurvitz, 1995), regardless if the etiology is idiopathic (Riskowski et al.,  
64 2012), due to diabetes (Mustapa et al., 2016; Vinik et al., 2017), or chemotherapy (Winters-Stone et  
65 al., 2017). The prevalence of PN in the US population for those over age 40 has been reported to be  
66 nearly 15% (Gregg et al., 2004). The importance of sensory information from plantar cutaneous  
67 mechanoreceptors for balance control has been shown in healthy individuals (Meyer et al., 2004a; b),  
68 with loss of such information in patients with PN likely leading to problems with gait and balance  
69 function and increased risk of falls (Menz et al., 2004; DeMott et al., 2007; Dixon et al., 2017;  
70 Lipsitz et al., 2018). The occurrence of fall-related injuries is up to 15 times higher in patients with  
71 diabetic PN than in healthy individuals (Cavanagh et al., 1992). Furthermore, the prevalence of  
72 polyneuropathy has been reported to be almost four times higher in persons older than 60 years and  
73 to independently contribute to functional impairments including difficulty walking and tendency to  
74 fall (Hoffman et al., 2015). Persons with polyneuropathy are more likely to fall and more often incur  
75 fall-related injuries (Hanewinkel et al., 2017). In a prospective study, 65% of older individuals with  
76 PN fell during a one-year period and 30% reported an injury from a fall (DeMott et al., 2007). In  
77 addition, low gait speed is a risk factor for falls (Studenski et al., 2003; Montero-Odasso et al., 2005),  
78 an important indicator of frailty (Kim et al., 2019) and a predictor of survival (Studenski et al., 2011).  
79 Although gait speed declines with healthy aging (Buracchio et al., 2010), the decline in individuals  
80 with progressive sensory loss may be four times as high (Lipsitz et al., 2018). Interestingly,  
81 interventions designed to improve gait speed may also increase survival (Hardy et al., 2007).

82  
83 Clinical treatment of gait and balance problems related to PN is mainly limited to the use of canes,  
84 walkers, physical therapy interventions and balance exercises (Richardson et al., 2001; Ganz and  
85 Latham, 2020) including Tai-Chi (Li and Manor, 2010; Manor et al., 2014; Quigley et al., 2014).  
86 Long-term use of bilateral ankle foot orthoses in elderly individuals with a history of falls showed  
87 positive changes in certain in-clinic static sway measures (Wang et al., 2019a), although long-term  
88 benefits related to fall rates and gait function appear limited (Wang et al., 2019b).

89  
90 Several review studies support the hypothesis that strength and balance training interventions can  
91 improve balance and reduce fall risk and falls in patients with PN (Ites et al., 2011; Tofthagen et al.,  
92 2012; Streckmann et al., 2014). The training, however, should be specific to balance (Bulat et al.,  
93 2007; Oddsson et al., 2007; Halvarsson et al., 2011; Akbari et al., 2012) because strength and/or  
94 endurance training in patients with PN appears to have less impact on balance (Streckmann et al.,  
95 2014). In addition, unless balance activities, including Tai Chi or balance therapies are conducted  
96 with sufficient intensity, frequency (Lipsitz et al., 2019) and specificity, benefits may be limited or  
97 absent (Kruse et al., 2010; Lipsitz et al., 2018; Lipsitz et al., 2019) leading to mixed outcomes.  
98 Furthermore, continued exercise is required to maintain benefits long-term (Wolf et al., 2001;  
99 Halvarsson et al., 2013; Melzer and Oddsson, 2013), although some improvements last up to six

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100 months (Allet et al., 2010). Guidelines regarding physical activity for older adults with mobility  
101 problems recommend a minimum of activity at least twice a week (Chodzko-Zajko et al., 2009).  
102 Some studies on patients with diabetic PN following a period of balance training 2-3 times /week  
103 over 6-12 weeks did show improved balance and reduced fall risk (Morrison et al., 2010; Morrison et  
104 al., 2018). However, there currently are no specific guidelines regarding frequency of balance  
105 exercises and even three times a week may be insufficient to see an improvement in balance function  
106 (Kruse et al., 2010). Consequently, there is a need for additional solutions to help improve gait and  
107 balance function in patients with PN.

108  
109 A growing body of literature on various sensory substitution and augmentation technologies suggest  
110 novel ways of improving gait and balance function in different populations of patients. The concept  
111 of sensory substitution related to brain plasticity was laid out by Bach-y-Rita and colleagues, initially  
112 for vision and the vestibular system (Bach-y-Rita et al., 1969; Bach-y-Rita, 2004) and other sensory  
113 systems (Tyler et al., 2003; Bach-y-Rita, 2004). Recent efforts include wearable systems showing  
114 benefits to patients with vestibular loss (Hegeman et al., 2005; Wall et al., 2009; Basta et al., 2011;  
115 Yamanaka et al., 2016), PN (Wall et al., 2012; Wrisley et al., 2018) and Parkinson's Disease (Rossi-  
116 Izquierdo et al., 2013; Lee et al., 2015). Combining wearable neurostimulation with balance therapy  
117 has shown benefits in patients with multiple sclerosis (Leonard et al., 2017), cerebellar ataxia (Cakrt  
118 et al., 2012), stroke (Badke et al., 2011) traumatic brain injury (Ptitto et al., 2020) and in-home  
119 balance therapy (Bao et al., 2018)

120  
121 In a randomized crossover trial, a recent study further supported findings from an earlier pilot study  
122 (Wall et al., 2012) and demonstrated meaningful short-term, in-clinic improvements in Functional  
123 Gait Assessment (FGA) scores and gait speed in subjects with PN using a wearable sensory  
124 neuroprosthesis (Koehler-McNicholas et al., 2019). The device (Walkasins®, RxFunction Inc., MN,  
125 USA, Figure 1) is an external lower limb sensory prosthesis designed to replace lost nerve function  
126 used for detection and signaling of foot pressure sensation in patients with PN. It provides gentle  
127 directional tactile stimuli (in the form of low-intensity vibrations) around the lower leg that reflect  
128 changes in foot pressure distribution measured with an instrumented Foot Pad in the shoe. The  
129 subject's nervous system senses these new tactile cues and incorporates them to improve gait and  
130 balance. Currently, effects of long-term daily use of Walkasins on clinical outcomes are unknown.  
131 The multi-site clinical trial, walk2Wellness, (NCT #03538756, [www.clinicaltrials.gov](http://www.clinicaltrials.gov)) investigates  
132 long-term, home-based use of Walkasins on clinical and patient-reported outcomes of balance and  
133 gait function, quality of life, physical activity, social participation, pain and fall rates. Data from the  
134 primary endpoint of the study at 10 weeks are reported here. We hypothesized that previously  
135 demonstrated short-term in-clinic improvements in FGA score by at least four points would be  
136 sustained long-term (Beninato et al., 2014; Koehler-McNicholas et al., 2019). Early data from the  
137 trial were presented in abstract form (Oddsson et al., 2019; Oddsson et al., 2020a).

138

## 139 2 Materials and Methods

### 140 2.1 Subject Recruitment

141 Human subject testing was approved according to the Declaration of Helsinki by Advarra IRB  
142 (formerly Quorum Review IRB), serving as the Institutional Review Board (IRB) of record for three  
143 of the participating sites under the study protocol for *walk2Wellness: Long-term Use Effects of*  
144 *Walkasins® Wearable Sensory Prosthesis on Gait Function, Balance-Confidence, and Social*  
145 *Participation*. The three sites include Baylor College of Medicine, Houston, TX; Hebrew SeniorLife,  
146 a Harvard Medical School Affiliate, Boston, MA; and M Health Fairview, Minneapolis, MN.  
147 Advarra IRB determined that Walkasins are a non-significant risk device because they do not meet  
148 the criteria of a significant risk device according to U.S. Food and Drug Administration regulations.  
149 The IRB Subcommittee, the Subcommittee on Research Safety, and the Research and Development  
150 Committee of the Minneapolis VA Health Care System (MVAHCS) also approved the trial. The  
151 study is registered on ClinicalTrials.gov (#NCT03538756). At the time this study began, Walkasins  
152 were available only for research purposes.

### 153 2.2 Inclusion and Exclusion Criteria

154 Inclusion criteria for the study were similar to Koehler-McNicholas et al. (Koehler-McNicholas et al.,  
155 2019): age 21-90 years; male or female; a formal diagnosis of sensory PN prior to participating in the  
156 study as indicated by subject's medical record or a signed letter by a physician; self-reported  
157 problems with balance; ability for transfers or ambulation on level surfaces at fixed cadence as  
158 assessed by trained study personnel; an Functional Gait Assessment (FGA) score <23, the cut-off  
159 score for high fall risk (Wrisley and Kumar, 2010); ability to understand and provide informed  
160 consent; foot size to allow the Walkasins device to function properly, and ability to complete all  
161 functional outcome measures without the use of an assistive device to ensure sufficient motor  
162 function. Subjects could use an assistive device at their own discretion during the trial. Subjects were  
163 excluded from participation if they were unable to perceive tactile stimuli from the Walkasins leg  
164 unit or used an ankle-foot orthosis for ambulation that prevented donning of the device. Subjects with  
165 any of the following conditions were also excluded: acute thrombophlebitis; deep vein thrombosis;  
166 untreated lymphedema; a lesion of any kind, swelling, infection, inflamed area of skin, or eruptions  
167 on the lower leg near placement of the device; foot or ankle fractures; or severe peripheral vascular  
168 disease. In addition, subjects with any musculoskeletal or other neurological conditions that would  
169 prohibit use of the device, as determined by a clinician, were excluded. Due to risk of overloading the  
170 pressure sensor Foot Pad, subjects weighing over 136 kg (300lbs) were excluded from participation.  
171 Furthermore, subjects were prohibited from initiating any balance training (e.g., Tai-Chi etc.) or  
172 balance-related therapy during the ten weeks of the trial. Subjects were not systematically provided  
173 information about changes in any outcomes scores or changes in their performance throughout the 10  
174 weeks of the trial, nor did study personnel monitor outcomes during the study. Potential subjects  
175 responded to announcements that specifically targeted individuals with PN and balance problems, or  
176 they were referred by clinicians who were familiar with the study and believed them to be good  
177 candidates for the trial.

### 178 2.3 Study Procedures

179 All participants signed IRB-approved consent forms prior to the initiation of study activities.  
180 Following the informed consent process, a study team member tested the subjects on both legs to  
181 determine whether they could feel the stimuli from the Walkasins Leg Unit (Figure 1). Subjects wore

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182 Walkasins on both feet. A small number of subjects who were unable to perceive the stimuli from the  
183 Walkasins Leg Unit (Figure 1) were excluded from participation in the study. Participants then  
184 completed a demographics and health screening questionnaire to assess common health issues related  
185 to neurological, musculoskeletal, cardiopulmonary disorders, and other systemic diseases along with  
186 information on their history of falls over the past six and twelve months and regular use of an  
187 assistive device (Koehler-McNicholas et al., 2019). Falls were defined according to the World Health  
188 Organization: “an event which results in a person coming to rest inadvertently on the ground or floor  
189 or other lower level”. Subjects enrolled in the study were instructed to wear the device as much as  
190 possible throughout their daily activities, indoors as well as outdoors. At each follow-up visit,  
191 participants were asked about changes in their health status and any falls and adverse events they  
192 experienced since the previous visit. During the baseline visit, participants also provided a list of  
193 their medications (medication name, indication, dose, and frequency), which was updated over the  
194 course of the study. Medications are a known risk factor for falling, based on side effects of  
195 medication use or drug interactions (Woolcott et al., 2009).

### 196 **2.4 Initial Assessments**

197 Subjects then completed the Activities-Specific Balance Confidence (ABC) Questionnaire, which  
198 measures levels of balance confidence in elderly persons. The ABC asks the question “How  
199 confident are you that you will not lose your balance or become unsteady” when performing 16  
200 different tasks (Powell and Myers, 1995). Subjects rated themselves on a scale from 0 to 100, and an  
201 average score was calculated across the 16 responses. An ABC score below 67% has been associated  
202 with high fall risk (Lajoie and Gallagher, 2004). In addition, subjects completed the Vestibular  
203 Activities of Daily Living Scale (VADL) (Cohen et al., 2000), which evaluates self-reported effects  
204 of vertigo and balance disorders on independence in everyday activities of daily living that are  
205 relevant for individuals living in the community. Individuals rate their level of functional ability for  
206 basic and instrumental activities of daily living on a scale from 1 (independent) to 10 (dependent),  
207 which incorporates the use of assistive devices.

208  
209 Following completion of the questionnaires, a study team member performed tactile and vibration  
210 sensation testing to document loss of sensation. Loss of sensation was tested with the Weinstein  
211 Enhanced Sensory Test (WEST) monofilament foot test (0.5g, 2g, 10g, 50g, and 200g) applied  
212 perpendicular to the skin at four test sites on the plantar surface of the foot, including the first, third,  
213 and fifth metatarsal heads as well as the great toe. Study personnel began testing with the 10g  
214 filament and used a smaller filament if the subject was sensate and a larger filament if the subject was  
215 insensate. The smallest filament the subject was able to feel was recorded (if none were felt this  
216 result was recorded as “none”). Vibration sensation was assessed with a Rydel-Seiffer tuning fork,  
217 which is a 128Hz tuning fork with end weights that convert the tuning fork from 128 to 64 Hz. The  
218 weights are scaled allowing a score 0-8 (lower scores indicating less sensation), allowing reliable  
219 quantitative vibratory testing. Scores were read from the black triangle and rounded to the nearest  
220 whole number. Vibration values  $\leq 4$  are categorized as abnormal at the first metatarsal joint  
221 (Kästenbauer et al., 2004). The tuning fork was applied firmly and perpendicular to the lateral aspect  
222 of the first metatarsophalangeal, lateral malleolus, and patella testing sites. The monofilament and  
223 vibration tests were repeated at the 10-week visit.

### 224 **2.5 Clinical Outcome Measures**

225 Upon completion of the monofilament and vibration sensation testing, subjects performed a series of  
226 functional outcome measures while wearing the device turned off (baseline). Tests were repeated at

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227 weeks 2, 6, and 10. Subjects could rest as needed during the clinical assessments. For study purposes  
228 the clinical outcomes were standardized and performed by study personnel who were trained by one  
229 of the investigators (DW). Observation visits were conducted periodically during the study to ensure  
230 standardization among the sites.

231  
232 **Functional Gait Assessment (FGA):** The FGA (Wrisley et al., 2004) is the recommended clinical  
233 outcome measure for walking balance based on current physical therapy Clinical Practice Guidelines  
234 for outcome measures for adults with neurologic conditions (Moore et al., 2018). It is a reliable and  
235 valid measure of gait function related to postural stability and has been shown to be effective in  
236 classifying fall risk in older adults and predicting unexplained falls in community-dwelling older  
237 adults (scores  $\leq 22/30$ ) (Wrisley et al., 2004; Wrisley and Kumar, 2010). It has also been validated in  
238 multiple neurological conditions (stroke, Parkinson's, vestibular conditions) (Lin et al., 2010; Leddy  
239 et al., 2011) and has less floor and ceiling effects than the similar Dynamic Gait Index (Lin et al.,  
240 2010). The FGA includes 10 different items that challenge gait balance where each item is scored  
241 from 0 to 3 (3 = normal, 2 = mild impairment, 1 = moderate impairment, 0 = severe impairment) with  
242 a maximum score of 30. An increase of  $\geq 4$  points is considered the Minimal Clinically Important  
243 Difference (MCID) for community-dwelling elderly individuals (Beninato et al., 2014). Subjects  
244 whose baseline FGA score was 23 or higher were excluded from further participation in the study.  
245 Subjects completed the FGA in a large open area with a 6-m (20-ft) walkway marked with tape  
246 according to published recommendations (Wrisley et al., 2004).

247  
248 **10-Meter Walk Test (10MWT):** The 10m-walk (Perera et al., 2006) is the recommended clinical  
249 outcome measure for walking speed based on current physical therapy Clinical Practice Guidelines  
250 for outcome measures for adults with neurologic conditions (Moore et al., 2018). It is routinely used  
251 in rehabilitation and has excellent reliability in multiple neurologic conditions (chronic stroke,  
252 traumatic brain injury, Parkinson's) (Hiengkaew et al., 2012). Gait speed has been found to be an  
253 important predictor of survival in older adults (Hardy et al., 2007), further emphasizing its  
254 importance as a clinical outcomes measure. Gait speed was assessed during the middle 6 meters of a  
255 10-meter-long pathway to allow for acceleration and deceleration, completed in one trial under two  
256 conditions: 1) walk at normal speed and 2) walk as fast as possible. An increase by 0.05 m/s is  
257 deemed "small meaningful" and 0.10 m/s as "substantial" (Perera et al., 2006). These are considered  
258 the MCID in the geriatric population (Perera et al., 2006).

259  
260 **Timed Up and Go (TUG):** The TUG (Mathias et al., 1986) is part of the CDC recommended  
261 STEADI test protocol for balance function (CDC, 2017). It is commonly used in rehabilitation and  
262 has excellent validity and reliability for elderly adults and has been shown to be effective in  
263 classifying community dwelling adults at risk for falls (Podsiadlo and Richardson, 1991; Shumway-  
264 Cook et al., 2000; Bischoff et al., 2003; CDC, 2017). From a seated position in a standard armchair,  
265 the subject is asked to do the following: 1) stand up from the chair, 2) walk at normal pace around a  
266 tape mark on the floor 10 feet from the chair, 3) turn, 4) walk back to the chair at a normal pace, and  
267 5) sit down again. Subjects were provided one practice trial that was not recorded followed by the  
268 recorded timed trial. The tester recorded the time from the command "Go" until the subject's  
269 buttocks returned to the chair when sitting. We used  $>12$ s as a cut-off for high fall risk (Bischoff et  
270 al., 2003; CDC, 2017). The Minimal Detectable Change (MDC) for older adults with type 2 diabetes  
271 has been reported to be 1s (Alfonso-Rosa et al., 2014).

272  
273 **4-Stage Balance Test:** The 4-Stage Balance Test is part of the Centers for Disease Control and  
274 Prevention (CDC)-recommended STEADI test protocol for balance function (CDC, 2017). It

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275 includes four gradually more challenging postures the subject is exposed to: 1) stand with feet side by  
276 side, 2) stand with feet in semi-tandem stance, 3) stand with feet in tandem stance, and 4) stand on  
277 one leg. Subjects were allowed upper extremity support to obtain the position and passed each level  
278 if they were able to hold the stance unsupported for 10 seconds. The assessment ended when subjects  
279 were unable to hold a stance for 10 seconds. The times for each position held was recorded and  
280 summed as a measure of overall performance. A fail of stances 1, 2, or 3 (i.e., total time < 30s)  
281 indicates high risk of falling (CDC, 2017).

### 282 **2.6 Learning Protocol**

283 As part of the baseline visit, subjects performed a standardized set of balance activities, once while  
284 wearing the device turned off and once while wearing it turned on (Koehler-McNicholas et al., 2019).  
285 Activities lasted approximately 10 minutes and included standing (two-leg standing, tandem  
286 standing, and one-legged standing) and walking (walking straight, turning right and left) at both  
287 normal and fast speeds. Activities were repeated with the eyes closed. During standing exercises  
288 subjects were challenged to explore their base of support in both mediolateral and anteroposterior  
289 directions and to notice the pattern of tactile stimuli when the device was turned on. During walking  
290 activities subjects were instructed to notice the pattern of tactile stimuli when the foot was in contact  
291 with the ground, how it matched their pace of walking, and the flow of tactile stimuli from step to  
292 step. Subjects were not instructed how to respond to the tactile stimuli from Walkasins instead, the  
293 activities focused on orientation and familiarization with the device.

### 294 **2.7 Participant Reported Outcomes**

295 At the baseline visit and at each follow-up visit at weeks 2, 6, and 10, subjects also completed the  
296 five subject-reported outcome measures described below:

297  
298 **Patient Health Questionnaire (PHQ-9):** The PHQ-9 (Kroenke et al., 2001) is a concise, self-  
299 administered tool for assessing depression. Commonly used for screening and diagnosis of  
300 depression, the PHQ-9 incorporates depression criteria according to the 4<sup>th</sup> edition of the Diagnostic  
301 and Statistical Manual of Mental Disorders (DSM-IV) with other leading major depressive  
302 symptoms.  
303

304 **PROMIS Pain Interference Short Form 6b** (Askew et al., 2016): The PROMIS Pain Interference  
305 instrument measures the self-reported impact of pain on relevant aspects of a person's life within the  
306 past seven days. Items capture the extent to which pain hinders social, cognitive, emotional, physical,  
307 and recreational activities. The Pain Interference short form is a global scale rather than disease  
308 specific.  
309

310 **PROMIS Numeric Rating Scale v1.0 - Pain Intensity Form 1a:** The PROMIS Pain Intensity  
311 instrument assesses reported average pain intensity on a scale from 0-10 with higher scores indicating  
312 greater levels of pains. The Pain Intensity short form is global rather than disease specific.  
313

314 **PROMIS Ability to Participate Short Form 8a:** The PROMIS Ability to Participate in Social  
315 Roles and Activities instrument (Hahn et al., 2016b) assesses the individual's perceived ability to  
316 perform usual social roles and activities. The measure does not use a designated time frame (e.g. over  
317 the past seven days), and higher scores represent fewer limitations (e.g., I have trouble doing all of  
318 my regular leisure activities with others).  
319

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320 **PROMIS Satisfaction with Participation in Social Roles Short Form 8a:** The PROMIS  
321 Satisfaction with Social Roles and Activities (Hahn et al., 2014; Hahn et al., 2016a) is a self-reported  
322 instrument to assess satisfaction with the ability to perform usual social roles and activities (e.g., “I  
323 am satisfied with my ability to do things for my family”).  
324 PROMIS scores are presented as T-scores, a standardized score with a mean of 50 (representing  
325 average for the US population) and a standard deviation of 10.

326  
327 **User Experience Survey:** At the 2 and 10-week visits, subjects completed a 10-question survey to  
328 collect information concerning their experience with the device. Subjects rated aspects of Walkasins  
329 use (e.g., donning and doffing, charging, etc.) on a 7-point Likert scale ranging from “Very Easy” to  
330 “Very Hard”. Subjects also rated their overall satisfaction with the device and were able to provide  
331 additional comments and feedback regarding their experience with the device. Between visits,  
332 subjects were asked to document their use of Walkasins on a calendar by marking the days they wore  
333 their Walkasins and for how many hours. The subject calendar was also used to facilitate  
334 documentation of falls that occurred over the course of the study (Hannan et al., 2010). Subjects were  
335 asked to return their calendars at their next study visit.

### 336 **2.8 Number of Subjects**

337 Sample size estimation was based on data from the recent study of a similar population of subjects  
338 (Koehler-McNicholas et al., 2019), showing a baseline average FGA score of 15.2 and standard  
339 deviation 4.8. The data was normally distributed according to the Shapiro-Wilk’s test. To detect a  
340 mean difference in pre- and post-FGA score  $\geq 4$  points, the Minimal Clinically Important Difference  
341 for community dwelling elderly individuals (Beninato et al., 2014), required at least 20 subjects using  
342 a significance level of 0.01 and a power of 0.8. Accounting for an expected ~20% drop-out rate  
343 (National Heart, 2020) target enrollment was set at 25 subjects ( $20/0.8=25$ ). Multiple sites were  
344 engaged in the trial to expand geographical, ethnical, and clinical variation in the data initially  
345 allowing each site to recruit up to 25 subjects. Due to the COVID-19 pandemic, the trial was  
346 interrupted and continued enrollment as well as in-clinic testing was halted. At this time, sufficient  
347 overall statistical power based on the sample size calculation above has been achieved following  
348 enrollment of 52 subjects, well over the 20 subjects required to achieve statistical significance.  
349 Collection of participant-reported outcomes has continued through phone calls and the longer-term  
350 outcomes assessments as originally planned (at 26 and 52 weeks) are expected to continue.

### 351 **2.9 Statistical Analysis and Availability of Data**

352 Descriptive statistics were calculated and presented as mean and standard deviation of the mean.  
353 Variables were tested for normality using the Shapiro-Wilk’s test. The two-proportion Z-test was  
354 used to compare proportion-based measures. Subjects who reported falls in the previous six months  
355 (Pre-Fallers,  $n=30$ ) were analyzed separately from the remaining subjects (Pre-NonFallers,  $n=22$ ).  
356 Comparisons of baseline characteristics between Pre-Fallers and Pre-NonFallers were made with a t-  
357 test for independent samples or a Mann-Whitney U test if data was not normally distributed based on  
358 a Shapiro-Wilk’s test. Repeated measures analysis of variance (ANOVA) was performed for  
359 outcomes measured across the four assessment events, baseline, 2, 6 and 10 weeks. If the ANOVA  
360 was significant ( $p<0.05$ ), three pairwise comparisons were made using dependent t-tests between the  
361 baseline assessments and each of the 2, 6 and 10-week assessments. If the ANOVA was non-  
362 significant, no further comparisons were made. A Bonferroni’s adjustment of significance levels for  
363 correlated measures was applied, ranging from  $p<0.0167$  ( $0.05/3$  for three comparisons) for a full  
364 correction (non-correlated measures,  $r=0$ ) and  $p<0.05$  for perfectly correlated measures ( $r=1$ )



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365 (Uitenbroek, 1997). Effect sizes were calculated using Cohen's d (Lakens, 2013) and were  
366 interpreted according to recommendations by Cohen (Cohen, 1988) with 0.2 representing a small  
367 effect, 0.5 a medium effect, and 0.8 a large effect. Ninety-five percent confidence intervals of effect  
368 sizes were estimated according to Algina (Algina et al., 2005). Statistical analysis was performed  
369 using the Analysis-ToolPak module in Microsoft Excel 2016 and the Real Statistics Resource Pack  
370 software, release 6.8 (Zaiontz, 2020). Table 1 shows baseline characteristics of subjects enrolled in  
371 the study from the four different clinical sites. Subject data were pooled for the continued analysis  
372 presented here.  
373 Datasets from the current study are available upon request. The raw data supporting the conclusions  
374 of this article will be made available to qualified researchers, without undue reservation.  
375

## 376 3 Results

### 377 3.1 Enrollment and Allocation

378 The flow chart for the study is shown in Figure 2. Sixty-seven subjects were assessed for eligibility  
379 across the four participating sites. Their respective baseline characteristics are shown in Table 1. First  
380 enrollment occurred at the MVAHCS on 10/22/2018, followed by M Health Fairview/University of  
381 Minnesota on 10/23/2018, Baylor College of Medicine on 12/20/2018 and Marcus Institute/Harvard  
382 Medical School on 09/19/2019. The last enrollment occurred at Baylor College of Medicine on  
383 01/10/2020. Subjects across the four sites were pooled for the continued analysis presented here.  
384 Fifteen subjects were excluded from participation of which five had an FGA score higher than 22;  
385 two were unable to sense tactile stimuli from the device; two had neurological conditions that  
386 prevented device use; two were planning to start physical therapy treatment, one declined to  
387 participate and three for other reasons. Fifty-two subjects were enrolled for baseline assessment and  
388 allocated for the intervention. A total of seven subjects discontinued participation, four subjects at the  
389 two-week assessment (two related to device use, one due to transportation issues, and one due to an  
390 unrelated adverse event, Figure 2), one ahead of the six-week assessment and two ahead of the 10-  
391 week assessment (due to device and study issues), respectively (Figure 2). A total of 45 subjects  
392 (87%) completed all in-clinic assessments from baseline to the 10-week endpoint.

### 393 3.2 Baseline Characteristics and Outcomes

394 Table 2 shows baseline characteristics of all enrolled participants (n=52), then separately for subjects  
395 who reported having fallen in the six months preceding the study (Pre-Faller, n=30) and those who  
396 did not report a fall (Pre-NonFaller, n=22). Overall, participants were elderly ( $74.4 \pm 8.7$  yrs.),  
397 overweight (BMI >25) and mostly male (79%). A majority used an assistive device (54%) and had  
398 fallen in the previous year (71%) or in the past six months (58%). Furthermore, a majority showed  
399 high fall risk based on low 4-Stage Balance Test outcomes (63% of subjects < 30s) (CDC, 2017) or  
400 low ABC scores (56% of subjects scored < 67%) (Lajoie and Gallagher, 2004). Twenty-five percent  
401 of participants had a normal gait speed less than 0.7 m/s (Montero-Odasso et al., 2005) and half of  
402 the participants performed the TUG slower than 12 s (CDC, 2017), the commonly used thresholds for  
403 high fall risk. The Pre-Faller group had a higher number of fall-risk factors as compared to the Pre-  
404 NonFaller group ( $5.3 \pm 1.0$ , vs.  $3.5 \pm 1.3$ , respectively,  $p < 0.000001$ ). The baseline FGA score was  
405 statistically significantly lower in Pre-Faller ( $13.5 \pm 3.7$ ) as compared to Pre-NonFaller ( $16.7 \pm 3.6$ ,  
406  $p < 0.004$ ). There was no difference in normal gait speed between the two groups ( $p = 0.12$ ), although  
407 fast gait speed was higher in the Pre-NonFaller ( $1.41 \pm 0.35$  m/s) as compared to the Pre-Faller  
408 subjects ( $1.13 \pm 0.34$  m/s,  $p < 0.006$ ). Furthermore, TUG times were significantly slower in the Pre-  
409 Faller group compared to the Pre-NonFaller ( $14.7 \pm 6.3$ s and  $12.0 \pm 2.9$ , respectively,  $p < 0.05$ ).

410  
411 The ABC score was higher in the Pre-NonFaller compared to the Pre-Faller group, although the  
412 difference was not statistically significant ( $66.0 \pm 19.7$  vs.  $57.0 \pm 15.2$ , respectively,  $p = 0.07$ ). The  
413 VADL score was marginally lower in the Pre-NonFaller group ( $3.29 \pm 1.02$ , vs.  $3.94 \pm 1.04$ ,  $p < 0.03$ ).  
414 Pain scores were similar for the two groups ( $2.6 \pm 2.1$  vs.  $2.9 \pm 2.4$ ). The PHQ-9 score was slightly  
415 higher in the Pre-Faller group, although the difference was not statistically significant ( $p = 0.11$ ).  
416 PROMIS outcome scores for “Pain Interference,” “Satisfaction with Social Roles,” and “Ability to  
417 Participate” (Table 2) showed mean values around 50 for both groups, which is considered average  
418 for the US population (Askew et al., 2016; Hahn et al., 2016a; Hahn et al., 2016b). Any differences  
419 were well within 10, which is one standard deviation of these measures in the US population (Table  
420 2) (Askew et al., 2016; Hahn et al., 2016a; Hahn et al., 2016b).

### 421 **3.3 Chronic Conditions and Medication Use**

422 Table 3 shows self-reported chronic conditions and medication use for subjects enrolled in the study.  
423 On average, subjects reported having  $8.2 \pm 3.3$  chronic conditions. All subjects had a diagnosis of PN  
424 either in their medical chart or provided in a letter signed by their physician. Most subjects reported  
425 having neuropathic pain in their feet (73%) as well hypertension (63%) and half of participants  
426 reported having chronic back pain. All subjects reported having difficulty with walking and balance.  
427 The Pre-Faller group reported a higher incidence of cancer as a chronic condition than the Pre-  
428 NonFaller group (43% vs. 14%, respectively,  $p < 0.03$ ). Falls in the 12 months preceding study  
429 participation were reported by all the Pre-Faller participants (i.e. reporting falls over the past 12 and  
430 six months) versus by seven of the 22 in the Pre-NonFaller group (i.e. reporting falls over the past 12  
431 but not six months) ( $p < 0.00001$ ). Ninety percent of the falls reported in the 7-12 months preceding  
432 the study were reported by the Pre-Faller participants ( $p < 0.000001$ ). Overall, participants reported  
433 taking one non-prescription medication and eight (median) prescription medications of which three  
434 are known to cause potential balance issues and increase the risk of falling (Woolcott et al., 2009).  
435 Medication use was similar between the Pre-Faller and Pre-NonFaller groups (Table 3).

### 436 **3.4 Clinical Outcomes**

437 Table 4 shows clinical outcomes for the 45 subjects who completed assessments at baseline, 2, 6 and  
438 10 weeks. For all subjects, repeated measures ANOVA showed highly statistically significant  
439 differences across the assessment events for all subjects and all clinical outcomes ( $0.00001 < p <$   
440  $0.01$ ) except for the 4-Stage Balance Test, which was not statistically significant ( $p = 0.23$ , Table 4  
441 ANOVA column). Further pairwise comparisons following statistically significant ANOVA showed  
442 highly statistically significant differences between the baseline assessment and the 2, 6, and 10-week  
443 assessments, respectively, for the FGA score and normal gait speed and between baseline and 6 and  
444 10 weeks, respectively, for fast gait speed and the TUG scores. Cohen's d effect size calculated  
445 between the baseline and 10-week endpoint was large for FGA (0.92, FGA change from 15.0 to 19.1)  
446 and small to medium for normal gait speed (0.42, 0.86m/s to 0.95m/s), fast gait speed (0.27, 1.24 m/s  
447 to 1.33 m/s) and the TUG (0.28, 13.8 s to 12.5 s, Table 4).

448  
449 Both the Pre-Faller and Pre-NonFaller groups increased their FGA scores from baseline to the 2-, 6-,  
450 and 10-week assessments, respectively ( $p < 0.00016$ ). The Pre-Faller group had lower FGA scores  
451 both at baseline as compared to the Pre-NonFaller (13.5 vs. 16.9) and at the 10-week assessment  
452 (16.8 vs. 22.0). Effect sizes for FGA changes for both groups were large, although higher in the Pre-  
453 NonFaller group compared to the Pre-Faller group (Cohen's d 1.38 vs 0.82, respectively). Similarly,  
454 normal gait speed increased for both groups although the effect size was larger in the Pre-NonFaller  
455 group (Cohen's d 0.74 vs. 0.28, respectively). Interestingly, fast gait speed only improved in the Pre-  
456 Faller group from 1.09 m/s at baseline to 1.17 m/s at 10 weeks ( $p < 0.015$ , Table 4) although effect  
457 size was small (Cohen's d 0.27). There was an overall statistically significant change in TUG for the  
458 Pre-Faller group (ANOVA,  $p < 0.025$ ) although none of the pairwise comparisons reached statistical  
459 significance required after Bonferroni correction ( $0.047 < p < 0.14$ ). The overall ANOVA for TUG in  
460 the Pre-NonFaller group was not statistically significant ( $p = 0.49$ , Table 4).

### 461 **3.5 Participant Reported Outcomes, Sensation Tests, and Device Use**

462 Patient reported outcomes for the 45 subjects who completed all assessments are shown in Table 5 as  
463 well as for the Pre-Faller and Pre-NonFaller groups. For all subjects, there was an overall significant  
464 ANOVA for the VADL score ( $p < 0.044$ ) although none of the pairwise comparisons reached

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465 statistical significance following Bonferroni correction ( $0.053 < p < 0.99$ ). There were no other  
466 statistically significant differences across all subjects during the 10-week period.

467  
468 Table 5 shows and data from vibration sensation testing using the Rydel-Seiffer graduated tuning  
469 fork for all subjects. There were no differences in vibration sensation between Pre-Faller and Pre-  
470 NonFaller and no differences between baseline and 10-week assessments. Vibration sensitivity  
471 showed bilateral symmetry across the three sites tested, right and left patella, lateral malleolus and  
472 first metatarsophalangeal joints, respectively. There was a gradual proximal to distal decrease in  
473 vibration sensitivity across the three sites from 4.3-4.4 proximally and 2.0 distally based on the 0-8  
474 Rydel-Seiffer scale (Table 5). Similarly, there was bilateral symmetry for the WEST monofilament  
475 sensitivity test. At baseline, the median for the monofilament test was 50g for both feet and across all  
476 four anatomical test sites, the first, third, and fifth metatarsal heads as well as the great toe. This was  
477 similar at the 10-week assessment with the exception for the first metatarsals of both feet where the  
478 median monofilament increased to 200g.

479  
480 In the Pre-Faller subgroup, there were no overall statistically significant differences for any of the  
481 participant reported outcomes across the 10-week period (Table 5). For the Pre-NonFaller group,  
482 there was a statistically significant difference in the PROMIS “Ability to Participate” score at two  
483 weeks (ANOVA,  $p < 0.04$ ,  $49.7 \pm 7.1$  to  $53.7 \pm 7.3$ ,  $p < 0.02$ , Table 5). The improvement appeared  
484 maintained at six ( $52.8 \pm 7.6$ ) and 10 weeks ( $53.7 \pm 8.4$ ) although it did not fully reach statistical  
485 significance ( $p < 0.06$ ). None of the other participant reported outcomes for the Pre-NonFaller group  
486 were statistically different across the 10-week period (Table 5). Subjects reported using the device on  
487 average  $5.5 \pm 1.4$  days/week (range 3.5-7.0) for a total of  $36.1 \pm 14.9$  hours/week (range 5.3-56.0).

### 488 3.6 Falls Assessment

489 Parameters related to falls and fall risk assessed at baseline and throughout the 10 weeks are shown  
490 in Table 6. Overall, after 10 weeks, 13 of the 45 subjects had achieved FGA scores higher than 22,  
491 the cut-off for normal fall risk (Wrisley and Kumar, 2010). Four of these subjects were part of the  
492 Pre-Faller subgroup and nine were from the Pre-NonFaller group. Subjects reported a total of 62 falls  
493 in the six months prior to the study. During the 10-week study period, 17 falls were reported, 13 of  
494 which occurred in the Pre-Faller group and four in the Pre-NonFaller group (Table 6). Sixteen of the  
495 25 Pre-Fallers did not fall during the 10-week period of the trial. There was a non-significant  
496 decrease in fall rate across all subjects (from 7.7 to 5.4 falls/1000 patient days,  $p < 0.27$ ). In the Pre-  
497 Faller group, there was a 46% statistically significant decrease in fall rate (from 13.8 to 7.4 falls per  
498 1000 patient days,  $p < 0.014$ ). The Pre-NonFaller group showed a smaller non-significant increase in  
499 fall rate (from 0 to 2.9 falls per 1000 patient days,  $p = 0.125$ ). This increase was based on one fall each  
500 by four subjects who had not fallen in the prior six months (Table 6). There was a statistically  
501 significant decrease in the number of fall risk factors (Table 6) from baseline to 10 weeks across all  
502 subjects (from 4.2 to 3.8 fall risk factors,  $p < 0.047$ ). This decrease was larger and statistically  
503 significant in the Pre-Faller group (from 5.1 to 4.3 fall risk factors,  $p < 0.023$ ). There was no change in  
504 the number of fall risk factors in the Pre-NonFaller group ( $p = 0.76$ , Table 6).

505

## 506 4 Discussion

### 507 4.1 Key Findings

508 Results from this multi-site clinical trial supported our *a priori* hypothesis that patients with gait and  
509 balance problems due to sensory PN and high risk of falls would show clinically meaningful  
510 improvements of gait and dynamic balance function after 10 weeks of using a wearable sensory  
511 neuroprosthesis, confirming previously demonstrated in-clinic findings in a randomized controlled  
512 cross-over trial (Koehler-McNicholas et al., 2019). Overall, the mean FGA score improved from 15.0  
513 at baseline to 19.1 at 10 weeks across all subjects (Table 4), beyond the MCID for the FGA  
514 (Beninato et al., 2014). Thirteen subjects reached normal fall risk status showing an FGA score  
515 higher than 22 (Wrisley and Kumar, 2010) after 10 weeks of device use. Both normal and fast gait  
516 speed improved overall by 0.09m/s, near what is considered substantial change (0.10m/s) for older  
517 adults (Perera et al., 2006). Across both groups, TUG improved from 13.8 s to 12.5 s, which is  
518 beyond the MDC for older adults with type 2 diabetes (Alfonso-Rosa et al., 2014). Effect sizes  
519 ranged from large for FGA scores (Cohen's d, 0.92) to small for fast gait speed and TUG (0.27 and  
520 0.28, respectively).

521  
522 As expected, vibratory sensation did not improve during the trial suggesting new sensory information  
523 from the device provided relevant input to improve function. Although both Pre-NonFallers and Pre-  
524 Fallers showed improvements, effect sizes were larger in the Pre-NonFaller group for FGA and  
525 normal gait speed while only the Pre-Faller group showed a statistically significant improvement in  
526 fast gait speed with an effect size of 0.27. The increase in fast gait speed from 1.41 m/s to 1.52 m/s in  
527 the Pre-NonFaller group did not reach statistical significance (ANOVA main effect,  $p=0.10$ ),  
528 although such gait speeds are considered in the high range of elderly community ambulators  
529 (Middleton et al., 2015). Interestingly, the 4-Stage Balance measure, an indicator of static balance,  
530 did not improve significantly over the 10-week period in either of the two subgroups although our  
531 recent in-clinic study (Koehler-McNicholas et al., 2019) found a statistically significant improvement  
532 in this measure in a group of PN patients. One important difference between these two groups may be  
533 a slightly lower baseline static balance performance in the first cohort, a mean of 22.2 s versus 26.2 s  
534 in the current one. The first group improved their performance in clinic to a mean of 27.6 s ( $p<0.001$ )  
535 while they improved to a nearly identical 27.8 s (n.s.) in the current study. It may be that further  
536 improvement of static balance performance would require some additional training challenge in  
537 addition to device use (e.g. Romberg and sharpened Romberg types of activities) and simply wearing  
538 the device daily does not sufficiently challenge the static balance ability assessed by the 4-Stage  
539 Balance Test.

### 540 4.2 Physical Intervention versus Sensory Substitution

541 To our knowledge, this is the first trial where a cohort of subjects with gait and balance problems  
542 related to PN have worn a sensory prosthetic device of this kind in the community and on a regular  
543 basis. Other wearable neuromodulation technologies have been used as a treatment modality in a  
544 home setting, although typically only worn in conjunction with a home therapy program for balance  
545 and mobility in different categories of subjects, e.g., multiple sclerosis (Leonard et al., 2017) and  
546 healthy elderly (Bao et al., 2018). A recent case study of a patient with PN wearing Walkasins for a  
547 year (Wrisley et al., 2018), found dramatic improvements in gait and balance outcomes when daily  
548 continuous device use was combined with balance therapy. The patient had received balance therapy  
549 twice a week for over five months prior to using Walkasins and no longer noticed any further  
550 improvements (Wrisley et al., 2018). In the current study, in an attempt to isolate the effect of long-

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551 term device use on clinical outcomes, subjects were instructed to wear the device as much as possible  
552 and were not allowed to participate in any additional balance training or therapy. Furthermore, they  
553 were not systematically informed of any changes in their outcomes or performance, which they  
554 would normally receive in regular clinical care. Still, improvements in clinical outcomes were similar  
555 to those reported after various balance intervention programs conducted over comparable time  
556 periods up to 12 weeks in similar patient populations (Shumway-Cook et al., 1997; Wolf et al., 2001;  
557 Li et al., 2005; Manor et al., 2014), or even longer up to six months and nearly a year (Wolf et al.,  
558 2003; Li et al., 2005; Li and Manor, 2010).

559  
560 Interestingly, two systematic reviews of interventions specifically for patients with diabetic PN gave  
561 lower extremity strengthening only a fair recommendation while other interventions showed  
562 insufficient evidence to increase function (Ites et al., 2011; Tofthagen et al., 2012). More recently,  
563 improvement in function in patients with PN following specific task-oriented training has been  
564 shown (Salsabili et al., 2015). Consequently, it may be particularly difficult to enhance gait and  
565 balance function in individuals with PN using physical therapy or balance training activities alone,  
566 possibly because these interventions do not replace lost somatosensory input. Furthermore, effects of  
567 a training or therapy program on gait and balance function are likely due to different mechanisms  
568 than the use of a sensory substitution device.

569  
570 For training/therapy programs to be effective, well known principles of training and exercise  
571 physiology must be adhered to (Oddsson et al., 2007) ensuring that sensorimotor systems are  
572 sufficiently challenged to adapt and improve their capabilities leading to improved muscle function  
573 and neuromotor coordination. However, patients with PN have lost important cutaneous afferent  
574 systems that typically would not be affected by such interventions. Instead, improvements related to  
575 use of Walkasins seen in the current study are most likely due to participants receiving new tactile  
576 balance stimuli that are relevant for gait and balance and therefore become integrated into their  
577 neuromotor control and movement repertoire. Subjects in the current study received hundreds of such  
578 stimuli per hour from the device during their regular standing and walking activities throughout the  
579 day.

580  
581 Consequently, we hypothesize that any balance-related therapy or training activity in conjunction  
582 with wearing the device would provide an additive effect to overall function and balance outcomes.  
583 This hypothesis is supported by our recent case study (Wrisley et al., 2018) as well as our previous  
584 in-clinic study where subjects following a baseline assessment were randomized to either wearing the  
585 device turned on or turned off while performing a brief 10-15 min standardized balance activity  
586 session with a physical therapist (Koehler-McNicholas et al., 2019). Ten of 15 subjects in the on  
587 group increased their FGA scores by at least 4 points compared to five of 16 in the off group  
588 ( $p < 0.05$ ). Furthermore, seven of 15 subjects in the on group increased gait speed by  $> 0.13$  m/s  
589 compared to 3 of 16 in the off group ( $p < 0.05$ ) (Koehler-McNicholas et al., 2019).

### 590 **4.3 The Importance of Gait Speed**

591 Gait speed is a powerful indicator of overall health and survival in the elderly population and  
592 improving gait speed is an important therapeutic goal. Based on a large population study, Studenski  
593 et al. (Studenski et al., 2011) found that gait speed, age, and gender predicted survival as well as  
594 factors related to chronic conditions, smoking history, blood pressure, and hospitalization. In fact,  
595 improvement in gait speed by 0.10 m/s was found to predict better survival in older adults (Hardy et  
596 al., 2007). Furthermore, while each decrease in gait speed by 0.10 m/s has been associated with longer  
597 hospital stays and higher healthcare costs, each 0.10 m/s per year increase in gait speed has been

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598 shown to be predictive of shorter hospital stays and healthcare cost reduction (Purser et al., 2005)  
599 further emphasizing the importance of gait speed as a relevant health indicator and vital sign  
600 (Middleton et al., 2015).

601  
602 Healthy aging is associated with an annual decrease in gait speed by 0.013 m/s (Buracchio et al.,  
603 2010). However, it is well known that individuals with PN walk slower than their healthy counterparts  
604 (Menz et al., 2004; Lipsitz et al., 2018), likely as an adapted strategy to maintain balance (Dingwell  
605 et al., 2000). In fact, subjects with peripheral sensory loss (Lipsitz et al., 2018) who were consistently  
606 impaired over five years showed a decline in gait speed of 0.23 m/s over that time period, i.e., 0.046  
607 m/s/yr., more than 3.5 times higher than reported by Buracchio in healthy aging (Buracchio et al.,  
608 2010). Our current population of subjects with PN, who appear similar to the “impaired” category of  
609 community-dwelling older individuals in Lipsitz et al. (Lipsitz et al., 2018), showed an increase in  
610 gait speed of 0.09 m/s following 10 weeks of use of the Walkasins device, corresponding to an  
611 annual rate of 0.47 m/s. Interestingly, the Pre-Faller group increased both their normal and fast gait  
612 speed although the effect size was smaller compared to the Pre-NonFaller group who improved only  
613 their normal gait speed.

### 614 **4.4 Plantar Sensation and Balance Control**

615 The improvement in gait speed and function from wearing Walkasins may be interpreted from our  
616 understanding of the sensorimotor control of human locomotion and balance. When subjects with PN  
617 perform gait and balance activities, sensory information related to foot pressure is either completely  
618 absent or at least distorted and, therefore, likely non-veridical; and it is unlikely that remaining  
619 balance-related somatosensory information can sufficiently compensate, leading to decreased  
620 stability and increased risk of balance loss. Plantar cutaneous sensory information is important for  
621 standing balance (Meyer et al., 2004b; Strzalkowski et al., 2018) gait stability (Zehr et al., 2014)  
622 signaling stance limb placement and withdrawal to facilitate phase-dependent modulation of  
623 controlling reflex responses (Zehr and Stein, 1999) as well as when responding to balance  
624 perturbations (Meyer et al., 2004a). Hlavacka et al. (Hlavacka et al., 1995) stated that an internal  
625 representation of the body vertical requires integration of somatosensory and vestibular inputs, later  
626 emphasized by Bronstein who concluded that somatosensory information has a “prominent role” in  
627 verticality perception, which is crucial for optimal balance control (Bronstein, 1999). Marsden et al.  
628 (Marsden et al., 2003) concluded that the processing of vestibular information is influenced by load-  
629 related afferent feedback for control of balance.

630  
631 The integration of somatosensory and vestibular information appears of particular importance for gait  
632 function during the double support phase following foot placement during walking (Bent et al.,  
633 2004), which is near the events when Walkasins provides tactile stimuli. Although of lesser fidelity  
634 than intact plantar sensation, the Walkasins device may provide sufficient and relevant sensory  
635 information that is veridical both during standing and walking activities by signaling out of balance  
636 events during standing as well as indicating stance and swing phases of gait, which can help improve  
637 gait and balance function. Furthermore, these tactile stimuli are provided just proximally to the  
638 original sensory loss and mainly along the same dermatomes representing the plantar surface of the  
639 foot possibly making it intuitive to integrate into functional behavior (Koehler-McNicholas et al.,  
640 2019) by providing relevant sensory information to spinal central pattern generators for locomotion  
641 (Guertin, 2012).

642  
643

#### 644 **4.5 Falls Data**

645 Although we noticed an encouraging decrease in fall rate as well as in the number of fall-risk factors  
646 in the Pre-faller subgroup (Table 6), a 10-week time period with a fairly small number of subjects is  
647 too short to draw any final conclusions related to prevention of falls. Continued evaluation of longer-  
648 term data from the walk2Wellness trial during continued use of the device is currently ongoing (26  
649 and 52 weeks) and will be reported at a future date. Interestingly, studies have found that effects of  
650 improved clinical gait and balance outcomes may lead to a delayed effect of fall reduction, which  
651 was reported following six months of Tai Chi (Li et al., 2004; Li et al., 2005) and also observed by  
652 Wolf et al. (Wolf et al., 1996; Wolf et al., 2003).

#### 653 **4.6 Participant Reported Outcomes**

654 There appeared to be none or only minimal changes in the self-report measures throughout the 10  
655 weeks of the trial (Table 5). Although this may seem counterintuitive, Richardson et al. (Richardson  
656 et al., 2001) reported significant improvements in clinical balance outcomes, but non-significant  
657 improvement in the ABC score following a strength and balance intervention for patients with PN.  
658 Similarly, an exercise intervention study for older adults found discrepancies between balance and  
659 ABC score improvements suggesting that the relationship between balance confidence and functional  
660 performance may not be well understood (Cyarto et al., 2008). In the current study, a lack of overall  
661 improvement in the ABC score may also be influenced by subject expectations, the short duration of  
662 study, or the time of the year as some subjects were enrolled in the winter months during snowy and  
663 icy conditions. Furthermore, results of the ABC balance confidence scores may also be viewed in the  
664 context of the subjects not being systematically informed of changes in clinical outcomes during the  
665 study, nor receiving any organized encouragement reflecting their performance.

666  
667 Interestingly, upon further investigation we observed differences between the overall pattern of  
668 improvement in clinical outcomes versus self-reported measures of balance confidence as illustrated  
669 in Figure 3. Clinical outcomes at 10 weeks showed similar improvement across the full range of  
670 baseline scores, indicated by a regression line between baseline and 10-week scores being near  
671 parallel with the line of unity as illustrated with the FGA scores in Figure 3 A. However, this was not  
672 the case for the balance confidence ABC-score as seen in Figure 3 B (similar observations were made  
673 for the VADL scores, not shown here). As can be seen, the regression line between baseline and 10-  
674 week ABC scores intersects the line of unity and it has a slope of 0.47 (Figure 3 B). Interestingly, the  
675 two lines intersect at the baseline value 67%, the published cut-off value for high fall risk (Lajoie and  
676 Gallagher, 2004).

677  
678 Subjects enrolled in the current study were all at high fall risk based on their FGA score  $\leq 22$  (Wrisley  
679 and Kumar, 2010) as well as a diagnosis of PN (Richardson and Hurvitz, 1995). Based on additional  
680 outcomes and baseline characteristics, subjects had on average more than four fall risk factors (Table  
681 1, Table 2, Table 6). Consequently, it could be argued that study participants with multiple  
682 impairments related to balance maybe “should not” have a balance confidence ABC score above 67%  
683 and those who report such scores are either overly confident and/or simply unaware of their true  
684 balance capabilities. Compellingly, subjects with greater balance confidence at baseline actually  
685 showed a decrease in their balance confidence during the study (from  $76.5 \pm 8.1$  to  $71.8 \pm 9.9$ ,  $p < 0.02$ )  
686 while subjects with a baseline ABC score  $< 67\%$  (in the range of high-fall risk) increased their  
687 balance confidence scores ( $49.9 \pm 12.5\%$  to  $59.3 \pm 15.1\%$ ,  $p < 0.01$ ).

688



## Wearable Sensory Neuroprosthesis for Balance

689 If we consider a simple ratio between ABC and FGA scores representing “amount” of balance  
690 confidence per FGA point, someone with 100% balance confidence and the maximum FGA score of  
691 30 would have a ratio of 3.3. A ratio between the established cut-offs for high fall risk for ABC and  
692 FGA scores, 67% and 22, respectively, represents a ratio of 3.0. At baseline in the current trial, the  
693 overly confident subjects had a ratio of  $5.1 \pm 1.3$ , versus  $3.6 \pm 1.1$  for the low confidence subjects. After  
694 10 weeks of device use, with increased FGA scores across the board, the ratio was  $3.8 \pm 1.4$  for the  
695 overly confident subjects versus  $3.4 \pm 1.0$  for the lower confidence subjects. It appears the overly  
696 confident subjects may have “normalized” their self-perception of their balance ability while the  
697 lower confidence subjects increased their ABC score proportionally to their improved FGA score and  
698 maintained a similar self-confidence to FGA ratio. Although the FGA and ABC capture different  
699 constructs related to balance, it may be of importance for clinicians to be aware of the potential  
700 discrepancy between a patient’s self-perception and actual functional performance when developing a  
701 plan of care targeting gait, balance function and fall prevention.

702  
703 The T-scores for baseline PROMIS measures (Pain Interference, Satisfaction Social Roles, Ability to  
704 Participate) were all close to 50, which was unexpected since it is considered the average for the US  
705 population (Hahn et al., 2014; Askew et al., 2016; Hahn et al., 2016a; Hahn et al., 2016b). We had  
706 expected these outcomes to deviate significantly in this complex clinical population. Consequently,  
707 any major changes in these measures should not be expected although a small statistically significant  
708 improvement in PROMIS Ability to Participate score, which remained through 10 weeks, was seen  
709 for the Pre-NonFaller sub-group from baseline to the 2-week assessment.

710  
711 Some additional trends in the patient reported outcomes of interest for further research were  
712 observed, especially some differences between the Pre-Faller and Pre-NonFaller group. The Pre-  
713 Faller group had a PHQ-9 score of 5.3 at baseline, >5 considered mild depression (Kroenke et al.,  
714 2001), which decreased to 3.9 at 6 weeks and reached 4.5 at 10 weeks, changes that nearly reached  
715 overall statistical significance ( $p=0.08$ ), and of minimal clinical relevance (Kroenke et al., 2001). It  
716 may be of interest to further investigate individuals with higher initial PHQ-9 scores to better  
717 understand this observation. In the Pre-NonFaller group, a non-significant ( $p=0.12$ ), increasing trend  
718 in PROMIS Satisfaction Social Roles scores and a near significant improvement in VADL score  
719 ( $p=0.08$ ) were seen. Finally, while VAS Pain scores were overall in the range of mild pain ( $\leq 3$ ) and  
720 remained steady throughout 10 weeks, pain scores appeared to trend slightly lower in the Pre-  
721 NonFaller group, although not statistically significant ( $p=0.10$ ) and not clinically meaningful. Here it  
722 may be of interest to further investigate individuals with higher initial pain levels, especially those  
723 with neuropathy-related foot pain by using a more disease-specific pain rating scale.

### 724 **4.7 Study Limitations**

725 There are several limitations to this trial. It is not blinded, lacks a control group and a placebo  
726 treatment. Unfortunately, it is not feasible to blind subjects from treatment in the current study since  
727 being able to feel the tactile stimuli from the device is an inclusion criterion. Using some form of  
728 random pattern stimuli as a sham may seem possible (Basta et al., 2011), although it is not known if  
729 such stimuli may have an effect of their own and it would not help address the question whether  
730 using the device as currently designed, according to principles of sensorimotor control of balance and  
731 gait, has an effect on gait and balance function. Consequently, the best placebo treatment would  
732 likely be wearing a device that is turned off. However, without using some form of deceit claiming  
733 the device is working although it cannot be felt, it would likely be difficult to recruit participants for  
734 such research and/or to ensure long-term compliance. In addition, incorporating a minimal  
735 stimulation amplitude as a sham, assuming it has no effect may be incorrect since studies

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736 implementing stochastic resonance using subsensory mechanical noise have demonstrated  
737 improvement in balance (Lipsitz et al., 2015). Furthermore, using a randomized control cross-over  
738 design, we recently demonstrated in-clinic improvements in clinical outcomes when the Walkasins  
739 device was worn and turned on as compared to turned off (Koehler-McNicholas et al., 2019).  
740 Consequently, we felt comfortable incorporating a single treatment arm design knowing the in-clinic  
741 effects. Furthermore, any placebo effects were likely decreased by not systematically informing  
742 subjects about any changes in outcomes and minimizing encouragement during interactions with  
743 subjects that could affect expectation and beliefs in the treatment (Finniss et al., 2010; Enck et al.,  
744 2013; Coste and Montel, 2017), and prohibiting any additional balance training/therapy intervention  
745 during the 10 weeks of the trial.

746  
747 If the effects in this study were placebo our findings should align with research findings on the  
748 placebo arm of randomized, placebo-controlled trials (Wartolowska et al., 2016). A systematic  
749 review of temporal changes in the placebo arm across 47 surgical randomized control trials found  
750 that effects size of subjective outcomes was large (0.64), while effect size of objective clinical  
751 outcomes was small (0.11) (Wartolowska et al., 2016). Furthermore, major differences in placebo-  
752 effect sizes have been reported with subject-reported self-perception effects being larger than  
753 observer-based ratings (Rief et al., 2009). On the contrary, effect sizes in the current study were large  
754 for the clinical outcomes and small for the self-reported outcomes, supporting the interpretation that  
755 effects were due to device use and not placebo. Further support of this view includes relatively high  
756 subject compliance and reported device use and, a low subject dropout rate as well as the sustained  
757 duration and continued gradual improvement in clinical outcomes throughout the 10-week period. An  
758 additional weakness includes enrollment of mostly male subjects, partly due to nearly half of the  
759 subjects being Veterans, who especially in this older generation are predominantly male. Strengths of  
760 this trial include involvement of multiple sites across different geographies with different assessors at  
761 different clinics limiting confounding balance interventions, and the use of standardized objective  
762 clinical outcome measures.

## 763 **5 Conclusion**

764 A wearable sensory neuroprosthesis may provide a new way to treat gait and balance problems and  
765 manage falls in high fall-risk patients with PN. Longer term data would be required to further  
766 investigate actual decreases in falls.

## 767 **6 Acknowledgments**

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775 et al., 2020b).

## 776 **7 Contribution to the Field Statement**

777 Peripheral neuropathy is a condition affecting over 20 Million individuals in the US alone that causes  
778 damage to nerves in the peripheral nervous system. Peripheral neuropathy is often related to diabetes,

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779 chemotherapy treatment or has unknown causes. Symptoms of the disease that involve numbness and  
780 loss of sensation in the feet often lead to problems with gait and balance and a high risk of falls. We  
781 report results from the multi-site clinical trial, walk2Wellness, that has investigated long-term effects  
782 of daily use of a new wearable sensory neuroprosthesis on gait function, balance, fall rates, and  
783 quality of life in a group of peripheral neuropathy patients. The device (Walkasins®, RxFunction  
784 Inc., MN, USA) provides directional tactile stimuli around the ankle during standing and walking  
785 activities reflecting changes in foot pressure related to balance. Patients can then “feel” their feet in  
786 contact with the ground, notice body sway during standing replacing their lost afferent nerve  
787 function. Our results after 10 weeks of daily use show improved walking balance, speed of walking,  
788 ability to rise from a chair move around and sit down and an encouraging trend in lower fall rates.  
789 Also, participants with initial low self-confidence in their balance showed higher self-confidence.  
790

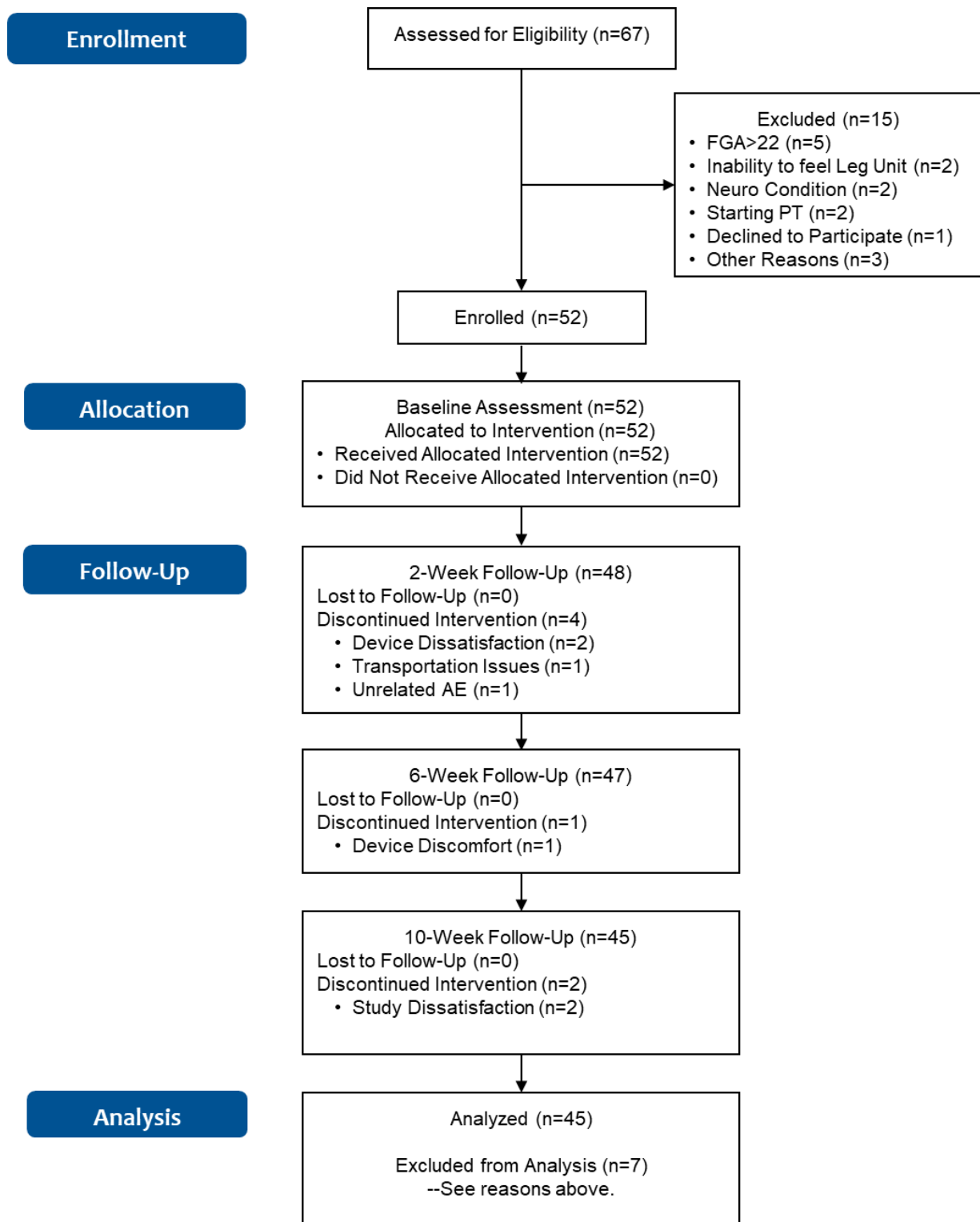
## Wearable Sensory Neuroprosthesis for Balance



791  
792 **Figure 1.** Picture of the Walkasins sensory neuroprosthesis device showing the pressure sensor embedded Foot Pad that  
793 is placed in the subject's shoe and connected to the Leg Unit that houses an embedded microprocessor with software,  
794 supporting electronics, a rechargeable battery, and four tactile stimulators placed around the lower leg. The system is  
795 worn bilaterally. Leg Unit and left Foot Pad shown

796  
797  
798

## Wearable Sensory Neuroprosthesis for Balance



799  
800 **Figure 2.** Flowchart of the study.  
801

## Wearable Sensory Neuroprosthesis for Balance

	n	Age (yrs)	Height (m)	Weight (kg)	#ChrD	FGA Score	Gait Speed Normal (m/s)	Gait Speed Fast (m/s)	TUG (s)	4-Stage Balance Test (s)
<b>VAMC</b>	20	74.7 (6.0)	1.76 (0.06)	96.9 (13.5)	9.8 (2.4)	14.8 (4.4)	0.80 (0.16)	1.2 (0.23)	14.7 (6.3)	25.0 (7.3)
<b>Baylor</b>	18	75.1 (11.7)	1.74 (0.08)	80.9 (18.1)	8.2 (3.0)	15.1 (4.2)	0.87 (0.25)	1.28 (0.39)	13.2 (5.2)	28.1 (8.2)
<b>M Health Fairview</b>	9	70.1 (7.8)	1.79 (0.12)	87.6 (10.5)	6.6 (4.1)	15.0 (3.2)	1.02 (0.28)	1.32 (0.27)	10.8 (2.3)	23.6 (5.2)
<b>Harvard</b>	5	78.2 (5.1)	1.71 (0.1)	95.0 (22.0)	5.2 (2.9)	14.0 (3.4)	0.77 (0.25)	1.07 (0.45)	15.0 (3.4)	28.3 (6.6)

802 **Table 1.** Baseline characteristics of subjects from the four different clinical sites enrolled in the study. Values represent  
803 Mean (Standard Deviation). #ChrD - Number of Chronic Diseases.  
804

## Wearable Sensory Neuroprosthesis for Balance

Baseline Assessment	All n=52	Pre-F n=30	Pre-NF n=22	p-level
Gender Female (n)	11 of 52 (21%)	9 of 30 (30%)	2 of 22 (10%)	0.069
Use of Assistive Device (n)	28 of 52 (54%)	19 of 30 (63%)	9 of 22 (41%)	0.11
Gait Speed Normal <0.7m/s (n)	13 of 52 (25%)	10 of 30 (33%)	3 of 22 (14%)	0.10
Timed Up and Go >12s (n)	26 of 52 (50%)	18 of 30 (60%)	8 of 22 (36%)	0.09
4-Stage Balance Test <30s (n)	33 of 52 (63%)	22 of 30 (73%)	11 of 22 (50%)	0.08
ABC Score <67% (n)	30 of 52 (56%)	20 of 30 (67%)	10 of 22 (45%)	0.13
Fallen in Last 6 Months (n)	30 of 52 (58%)	30 of 30 (100%)	0	n/a
Fallen in Last 12 Months (n)	37 of 52 (71%)	30 of 30 (100%)	7 of 22 (32%)	<b>&lt;0.00001</b>
Number of Falls 6 Months	65	65	0	n/a
Number of Falls 12 Months	121	109 of 121 (90%)	12 of 121 (10%)	<b>&lt;0.000001</b>
	Mean (SD) n=52	Mean (SD) n=30	Mean (SD) n=22	p-level
Age (yrs)	74.4 (8.7)	73.8 (9.1)	75.2 (8.2)	0.57
Height (m)	1.75 (0.08)	1.76 (0.09)	1.75 (0.07)	0.54
Weight (kg)	89.6 (16.8)	89.7 (17.8)	89.3 (15.8)	0.93
BMI (kg/m <sup>2</sup> )	29.1 (5.2)	29.0 (5.8)	29.2 (5.2)	0.92
FGA Score	14.9 (4.0)	13.5 (3.7)	16.7 (3.6)	<b>&lt;0.004</b>
Gait Speed, Normal (m/s)	0.86 (0.23)	0.81 (0.26)	0.92 (0.18)	0.12
Gait Speed, Fast (m/s)	1.25 (0.37)	1.13 (0.34)	1.41 (0.35)	<b>&lt;0.006</b>
TUG (s)	13.5 (5.3)	14.7 (6.3)	12.0 (2.9)	<b>&lt;0.05</b>
4-Stage Balance Test (s)	26.2 (7.3)	24.8 (6.3)	28.0 (8.3)	0.055
Fall-Risk Factors* (n of 7)	4.5 (1.5)	5.3 (1.0)	3.5 (1.3)	<b>&lt;0.000001</b>
ABC Score (%)	60.8 (17.6)	57.0 (15.2)	66.0 (19.7)	0.07
VADL Mean Score	3.66 (1.07)	3.94 (1.04)	3.29 (1.02)	<b>&lt;0.03</b>
VAS Pain Score (0-10)	2.7 (2.2)	2.6 (2.1)	2.9 (2.4)	0.67
PHQ-9	4.4 (3.8)	5.2 (4.3)	3.4 (3.8)	0.11
Pain Interference PROMIS® 6b	51.1 (8.0)	52.5 (8.1)	49.0 (8.1)	0.10
Satisfaction Social Roles PROMIS® 8a	50.4 (7.8)	49.1 (7.7)	52.1 (7.8)	0.13
Ability to Participate PROMIS® 8a	50.0 (7.2)	49.8 (7.1)	50.2 (7.2)	0.88

805 **Table 2.** Baseline characteristics of subjects enrolled in the study (n=52), then separately for subjects who reported  
 806 having fallen in the past six months (Pre-F) and those who did not (Pre-NF). Values shown are Mean (Standard  
 807 Deviation). Column p-level shows significance level for comparison between the Pre-F and Pre-NF groups. In bold if  
 808 p<0.05.

809 \*Fall-risk factors assessed in the current study included, recent history of falls (Tinetti and Kumar, 2010), PN diagnosis  
 810 (Richardson and Hurvitz, 1995), FGA score<23 (Wrisley and Kumar, 2010), TUG >12 s (CDC, 2017), 4-Stage Balance  
 811 Test<30s (CDC, 2017), Gait Speed <0.7m/s (Studenski et al., 2003; Montero-Odasso et al., 2005), ABC score <67%  
 812 (Lajoie and Gallagher, 2004).

813  
 814

### Wearable Sensory Neuroprosthesis for Balance

Baseline Assessment	All n=52	Pre-F n=30	Pre-NF n=22	p-level
Number of Chronic Conditions (n)	8.2 (3.3)	8.6 (3.2)	7.8 (3.4)	0.39
Peripheral Neuropathy (n)	52 (100%)	30 (100%)	22 (100%)	n/a
Numbness in Feet (n)	49 (94%)	30 (100%)	19 (86%)	<b>&lt;0.05</b>
Neuropathic Pain in Feet (n)	38 (73%)	22 (73%)	16 (73%)	0.96
Hypertension (n)	33 (63%)	19 (63%)	14 (64%)	0.98
Back Pain (n)	26 (50%)	16 (53%)	10 (45%)	0.57
Arthritis (n)	24 (46%)	15 (50%)	9 (41%)	0.52
Knee Dysfunction (n)	23 (44%)	14 (47%)	9 (41%)	0.68
Diabetes Diagnosis (n)	19 (37%)	9 (30%)	10 (45%)	0.25
Inner Ear Problems (n)	17 (33%)	9 (30%)	8 (36%)	0.63
Heart Disease (n)	16 (31%)	10 (33%)	6 (27%)	0.64
Neck Pain (n)	16 (31%)	9 (30%)	7 (32%)	0.89
Cancer (n)	16 (31%)	13 (43%)	3 (14%)	<b>&lt;0.03</b>
Lung Disease (n)	10 (19%)	7 (23%)	3 (14%)	0.38
Stroke (n)	9 (17%)	4 (13%)	5 (23%)	0.38
Osteoporosis(n)	10 (19%)	7 (23%)	3 (14%)	0.38
Seizures (n)	5 (10%)	3 (10%)	2 (9%)	0.91
Ankle Dysfunction (n)	5 (10%)	4 (13%)	1 (5%)	0.29
TMJ/Jaw Pain (n)	5 (10%)	2 (7%)	3 (14%)	0.40
Fainting (n)	5 (10%)	2 (7%)	3 (14%)	0.40
Migraines (n)	4 (8%)	2 (7%)	2 (9%)	0.75
Meningitis (n)	0	0	0	n/a
Other Conditions (n)	14 (27%)	11 (37%)	3 (14%)	0.06
Difficulty Walking/balance (n)	52 (100%)	30 (100%)	22 (100%)	n/a
	<b>Mean (SD) Median</b>	<b>Mean (SD)</b>	<b>Mean (SD)</b>	<b>p-level</b>
Prescription Medications (n)	8	8.5	7	0.50
Non-Prescription Medications (n)	1	1	1	n/a
Medications Associated with Falls (n)	3	3	3	n/a

815 **Table 3.** Self-reported chronic conditions as well as medication use for subjects enrolled in the study. Column p-level  
816 shows significance level for comparison between the Pre-F and Pre-NF groups. In bold if p<0.05.

817  
818



## Wearable Sensory Neuroprosthesis for Balance

<b>ALL</b>	<b>Baseline Mean (SD) n=45</b>	<b>2-week Mean (SD) n=45</b>	<b>6-week Mean (SD) n=45</b>	<b>10-week Mean (SD) n=45</b>	<b>ANOVA p-level</b>	<b>Cohen's d (95% CI's)</b>
FGA Score	15.0 (4.0)	18.3 (4.4) <b>&lt;0.000001</b>	18.5(4.4) <b>&lt;0.000001</b>	19.1 (5.2) <b>&lt;0.000001</b>	<b>&lt;0.00001</b>	0.92 (0.49, 1.35)
Gait Speed Normal (m/s)	0.86 (0.24)	0.92 (0.26) <b>&lt;0.002</b>	0.94 (0.25) <b>&lt;0.0001</b>	0.95 (0.24) <b>&lt;0.00005</b>	<b>&lt;0.00001</b>	0.42 (0.01, 0.82)
Gait Speed Fast (m/s)	1.24 (0.37)	1.27 (0.33) 0.30	1.30 (0.37) <b>&lt;0.016</b>	1.33 (0.38) <b>&lt;0.00168</b>	<b>&lt;0.013</b>	0.27 (-0.14,0.67)
TUG (s)	13.8 (5.5)	12.7 (4.2) 0.06	12.3 (4.2) <b>&lt;0.034 (0.69)</b> 0.0397*	12.5 (3.7) <b>&lt;0.012</b>	<b>&lt;0.01</b>	0.28 (-0.12, 0.68)
4-Stage Balance Test (s)	26.2 (7.1)	27.1 (7.7)	27.7 (7.7)	27.8 (6.8)	0.23	n/a
<b>Pre-Fallers</b>	<b>Baseline Mean (SD) n=25</b>	<b>2-week Mean (SD) n=25</b>	<b>6-week Mean (SD) n=25</b>	<b>10-week Mean (SD) n=25</b>	<b>p-level ANOVA</b>	<b>Cohen's d (95% CI's)</b>
FGA Score	13.5 (3.6)	16.6 (3.7) <b>&lt;0.0000005</b>	17.3 (4.1) <b>&lt;0.00002</b>	16.8 (4.9) <b>&lt;0.00016</b>	<b>&lt;0.00001</b>	0.82 (0.26, 1.39)
Gait Speed Normal (m/s)	0.79 (0.27)	0.85 (0.26) <b>&lt;0.022 (0.90)</b> 0.047*	0.89 (0.25) <b>&lt;0.0021</b>	0.86 (0.24) <b>&lt;0.016</b>	<b>&lt;0.0014</b>	0.28 (-0.27, 0.83)
Gait Speed Fast (m/s)	1.09 (0.33)	1.16 (0.30) <b>&lt;0.035 (0.88)</b> 0.046*	1.17 (0.32) <b>&lt;0.0165</b>	1.17 (0.35) <b>&lt;0.015</b>	<b>&lt;0.028</b>	0.27 (-0.28, 0.82)
TUG (s)	15.3 (6.6)	14.0 (4.6) 0.14	13.3 (3.8) 0.047	13.7 (4.2) 0.056	<b>&lt;0.025</b>	n/a
4-Stage Balance Test (s)	24.7 (5.5)	25.4 (7.8)	26.0 (7.9)	27.5 (6.1)	0.15	n/a
<b>Pre-NonFallers</b>	<b>Baseline Mean (SD) n=20</b>	<b>2-week Mean (SD) n=20</b>	<b>6-week Mean (SD) n=20</b>	<b>10-week Mean (SD) n=20</b>	<b>p-level ANOVA</b>	<b>Cohen's d (95% CI's)</b>
FGA Score	16.9 (3.6)	20.5 (4.4) <b>&lt;0.00009</b>	20.1 (4.3) <b>&lt;0.00004</b>	22.0 (4.0) <b>&lt;0.000004</b>	<b>&lt;0.0000001</b>	1.38 (0.70, 2.1)
Gait Speed Normal (m/s)	0.93 (0.17)	1.01 (0.22) <b>&lt;0.031 (0.78)</b> 0.043*	1.01 (0.24) <b>&lt;0.019 (0.84)</b> 0.045*	1.06 (0.20) <b>&lt;0.0004</b>	<b>&lt;0.0011</b>	0.74 (0.10, 1.37)
Gait Speed Fast (m/s)	1.41 (0.35)	1.42 (0.33)	1.43 (0.41)	1.52 (0.34)	0.10	n/a
TUG (s)	11.9 (2.9)	11.2 (3.2)	11.7 (5.0)	10.9 (2.2)	0.49	n/a
4-Stage Balance Test (s)	27.6 (8.5)	29.4 (7.1)	29.9 (7.1)	28.1 (7.7)	0.45	n/a

819 **Table 4.** Clinical outcomes for the 45 subjects completing all assessments for baseline, 2, 6 and 10 weeks as well as the  
820 subgroups of Pre-Fallers and Pre-NonFallers. Values in **bold** indicate statistical significance. ANOVA column shows  
821 significance levels of main effect from initial repeated measures ANOVA test. If significant ( $p < 0.05$ ), pairwise  
822 comparisons were made using three dependent t-tests between baseline and 2, 6 and 10-week assessments, respectively.  
823 Bonferroni's adjustment of significance levels for correlated measures was applied. As noted, values in *(italics)* indicate  
824 Pearson's correlation coefficient followed by the adjusted significance level required for an overall significance of 0.05 as  
825 marked with \*. If ANOVA was non-significant, no further comparisons were made. Cohen's d indicates effect size where  
826 0.2 is represents a small effect, 0.5 a medium effect, and 0.8 a large effect. Values in parenthesis show 95% confidence  
827 interval.  
828

## Wearable Sensory Neuroprosthesis for Balance

<b>ALL (n=45)</b>	<b>Baseline Mean (SD) n=45</b>	<b>2-week Mean (SD) n=45</b>	<b>6-week Mean (SD) n=45</b>	<b>10-week Mean (SD) n=45</b>	<b>ANOVA p-level</b>
ABC-Score (%)	61.4 (17.9)	65.0 (13.1)	64.2 (15.1)	65.1 (14.1)	0.36
VADL Mean Score	3.70 (1.09)	3.37 (0.86) 0.053	3.52 (0.99) 0.16	3.63 (0.93) 0.99	<b>&lt;0.044</b>
VAS Score (0-10)	2.8 (2.2)	2.5 (2.1)	2.5 (2.2)	2.6 (2.3)	0.31
PHQ-9	4.5 (3.9)	3.8 (3.5)	3.6 (3.8)	3.9 (4.5)	0.25
Pain Interference PROMIS® 6b	50.8 (7.9)	51.2 (8.1)	50.5 (8.9)	51.8 (8.5)	0.85
Satisfaction Social Roles PROMIS® 8a	50.2 (7.8)	52.1 (7.2)	51.7 (7.3)	52.1 (7.8)	0.10
Ability to Participate PROMIS® 8a	49.8 (7.3)	50.7 (6.4)	51.0 (7.1)	51.3 (8.1)	0.38
R 1st MTP Joint	2.0 (2.5)	n/a	n/a	2.0 (2.5)	n/a
R Lateral Malleolus	3.6 (2.7)	n/a	n/a	3.4 (2.6)	n/a
R Patella	4.5 (2.0)	n/a	n/a	4.5 (1.8)	n/a
L 1st MTP Joint	2.3 (2.6)	n/a	n/a	2.2 (2.7)	n/a
L Lateral Malleolus	3.7 (2.7)	n/a	n/a	3.6 (2.5)	n/a
L Patella	4.3 (2.1)	n/a	n/a	4.4 (1.6)	n/a
<b>Pre-Fallers (n=25)</b>	<b>Baseline Mean (SD)</b>	<b>2-week Mean (SD)</b>	<b>6-week Mean (SD)</b>	<b>10-week Mean (SD)</b>	<b>p-level</b>
ABC-Score (%)	57.7 (17.9)	61.5 (14.0)	61.8 (15.1)	61.2 (13.9)	0.29
VADL Mean Score	4.00 (1.13)	3.68 (0.90)	3.83 (1.01)	3.91 (0.97)	0.42
VAS Score (0-10)	2.5 (2.4)	2.5 (2.5)	2.8 (2.6)	2.6 (2.5)	0.55
PHQ-9	5.3 (3.9)	4.7 (3.3)	3.9 (3.3)	4.5 (3.5)	0.08
Pain Interference PROMIS® 6b	51.9 (8.3)	52.2 (8.5)	51.6 (9.9)	53.6 (8.0)	0.90
Satisfaction Social Roles PROMIS® 8a	49.1 (8.0)	49.9 (7.9)	49.2 (7.5)	49.6 (7.7)	0.68
Ability to Participate PROMIS® 8a	49.9 (7.5)	48.6 (5.8)	49.5 (6.8)	49.4 (8.0)	0.58
<b>Pre-NonFallers (n=20)</b>	<b>Baseline Mean (SD)</b>	<b>2-week Mean (SD)</b>	<b>6-week Mean (SD)</b>	<b>10-week Mean (SD)</b>	<b>p-level</b>
ABC-Score (%)	66.2 (18.0)	69.8 (11.9)	67.2 (15.1)	70.2 (14.6)	0.96
VADL Mean Score	3.32 (1.06)	2.94 (0.80)	3.11 (0.99)	3.28 (0.89)	0.08
VAS Score (0-10)	3.0 (2.0)	2.4 (1.5)	2.2 (1.7)	2.7 (2.0)	0.10
PHQ-9	3.5 (3.9)	2.6(3.7)	3.2 (4.4)	3.2 (5.6)	0.66
Pain Interference PROMIS® 6b	49.4 (7.6)	49.8 (7.6)	49.1 (7.6)	49.3 (9.1)	0.91
Satisfaction Social Roles PROMIS® 8a	51.7 (7.8)	55 .1 (6.4)	54.8 (7.0)	55.4 (8.0)	0.12
Ability to Participate PROMIS® 8a	49.7 (7.1)	53.7 (7.3) <b>&lt;0.02</b> (0.64) 0.038*	52.8 (7.6) 0.06	53.7 (8.4) 0.05	<b>&lt;0.041</b>

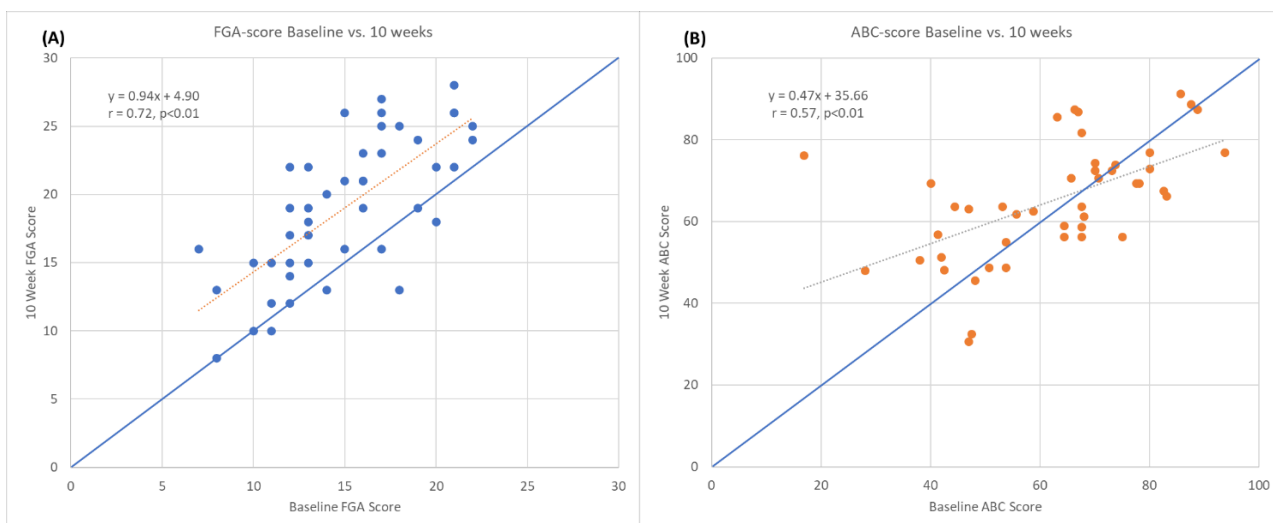
829 **Table 5.** Results from participant-reported outcomes and Rydel-Seiffer vibration sensation screening for the 45 subjects  
830 who completed all assessments. Data is shown separately for the group as a whole and for Pre-Fallers (having reported  
831 fallen in the previous 6 months) and Pre-NonFallers (no falls reported in the previous 6 months). Values in (*italics*)  
832 indicate Pearson's correlation coefficient followed by the Bonferroni adjusted significance level required for an overall  
833 significance of 0.05 as marked with \*. There were no differences in vibration sensation between Pre-Fallers and Pre-  
834 NonFallers and no differences between baseline and 10-week assessments.  
835

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<b>All (n=45)</b>	<b>Baseline</b>	<b>10 Weeks</b>	<b>p-level</b>
Number of Subjects FGA>22	0 of 45	13 of 45	n/a
#Falls (pre-6 mo & in study)	62	17	n/a
Fall Rate (pre-6mo & in study)	7.7	5.4	0.27*
#Fallers (pre-6mo & in study)	25	22	n/a
# Fall Risk Factors	4.2 (1.5)	3.8 (1.6)	<b>&lt;0.047</b>
<b>Pre-Fallers (n=25)</b>			
Number of Subjects FGA>22	0 of 25	4 of 25	n/a
#Falls (pre-6 mo & in study)	62	13	n/a
Fall Rate (pre-6mo & in study)	13.8	7.4	<b>&lt;0.014*</b>
#Fallers (pre-6mo & in study)	25	9	n/a
# Fall Risk Factors	5.1 (1.3)	4.3 (1.7)	<b>&lt;0.023</b>
<b>Pre-NonFallers (n=20)</b>			
Number of Subjects FGA>22	0 of 20	9 of 20	n/a
#Falls (pre-6 mo & in study)	0	4	n/a
Fall Rate (pre-6mo & in study)	0	2.9	0.125*
#Fallers (pre-6mo & in study)	0	4	n/a
# Fall Risk Factors	3.2 (1.8)	3.1 (1.7)	0.76

836 **Table 6.** Parameters related to falls and fall risk assessed at baseline and at 10 weeks. Fall rates are reported in number of  
837 falls per 1000 patient days. Fall risk factors are identified in Table 2. \*Wilcoxon Signed Rank test  
838

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840

841 **Figure 3.** Graphs showing baseline vs. 10-week FGA (A) and ABC scores (B). Markers above line of identity indicate  
842 higher scores at 10-week assessment. Notice line of regression for FGA scores is near parallel to line of identity  
843 indicating a similar increase across all baseline FGA scores. For ABC scores the line of regression intersects the line of  
844 identity near 67% indicating an increase for lower baseline ABC scores and a decrease for higher baseline ABC scores.

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